



TAL TECH

FLUID MECHANICS 1

LECTURE 2

Tamas Pardy
TalTech Lab-on-a-Chip

13.01.2022

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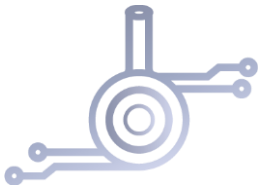
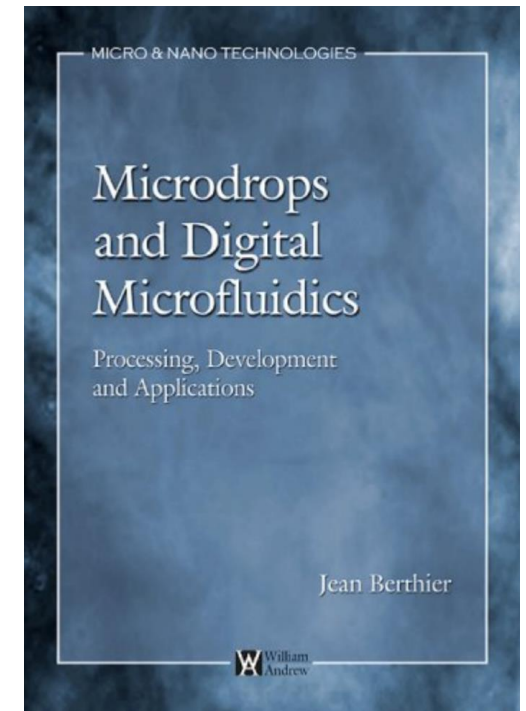
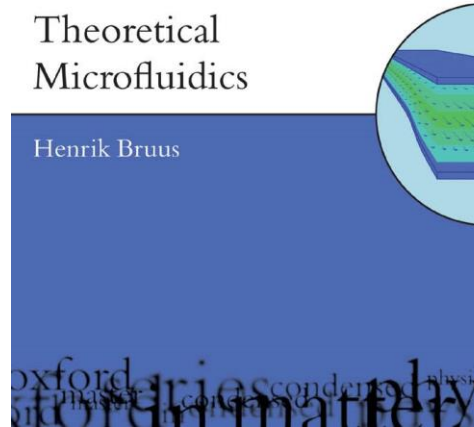
ADDITIONAL MATERIALS

- Theoretical Microfluidics
- **Henrik Bruus**
- ISBN: 9780199235087

- Microdrops and Digital Microfluidics
- **J. Berthier (editor)**
- ISBN: 978-0-8155-1544-9

- **Additional materials:**

- Nguyen, Nam-Trung, Steven T. Wereley, and Seyed Ali Mousavi Shaegh. Fundamentals and applications of microfluidics. Artech house, 2019.
- <https://www.youtube.com/watch?v=clVwKynHpB0>
- IEE1720 lecture 1 by Natalja Sleptsuk
- Tamas Pardy, "Development of a silicon-based digital microfluidics system for sample preparation tasks," Master Thesis, Faculty of IT, Peter Pazmany Catholic University, Budapest, 2013. (special thanks to the HAS and PPCU FIT)
- Utada, A. S., et al. "Dripping, jetting, drops, and wetting: The magic of microfluidics." *Mrs Bulletin* 32.9 (2007): 702-708.



OVERVIEW



SCALING LAWS

- Context
- Scaling of forces
- Effect of forces on microscale flows

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BASIC FLUID MECHANICS

- Continuum assumption
- Newtonian and non-newtonian fluids
- Flow types
- Diffusion
- Surface tension
- Contact angle

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INTRODUCTION TO DROPLETS

- Young's law
- Laplace law
- Capillary pressure
- Surfactants

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SUPERHYDROPHOBIC SURFACES

- Contact angle and wetting on micropatterned surfaces
- ...on rectangular micropillars
- ...in nature

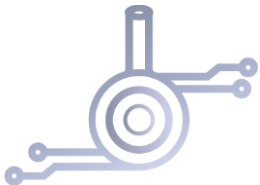
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PRESSURE AND FLOW RATE IN MICROCHANNELS

- Poisson equation
- Application to channels with...
- ...circular cross section
- ...rectangular cross section
- Flow control in microfluidics

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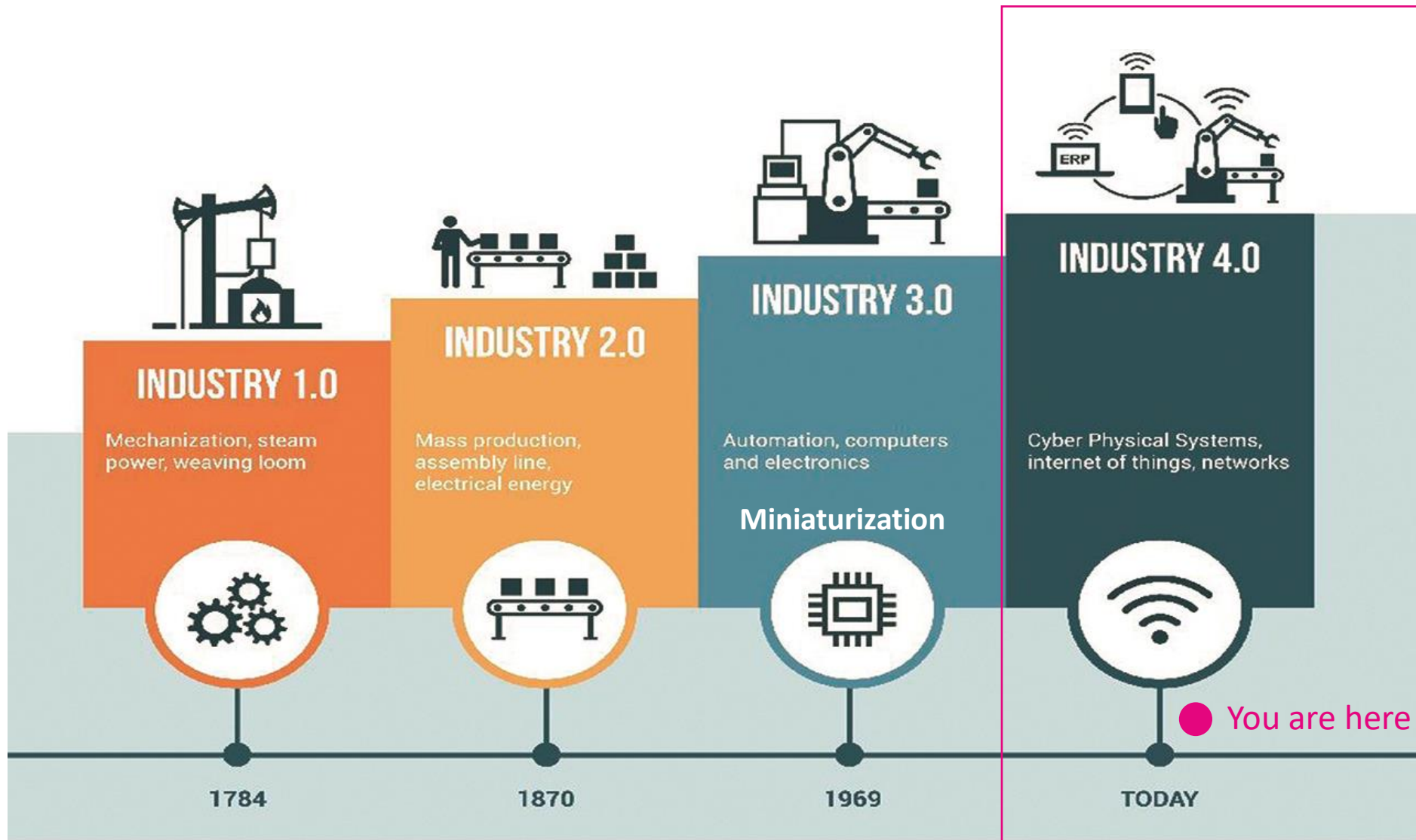


SCALING LAWS

- Context
- Scaling of forces
- Effect of forces on microscale flows

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TO PUT THINGS INTO PERSPECTIVE



Industry 5.0

- Human-centric
- Sustainable
- Resilient

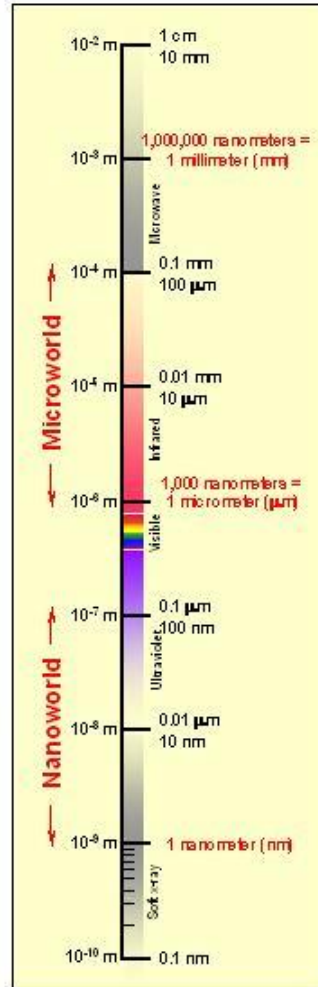
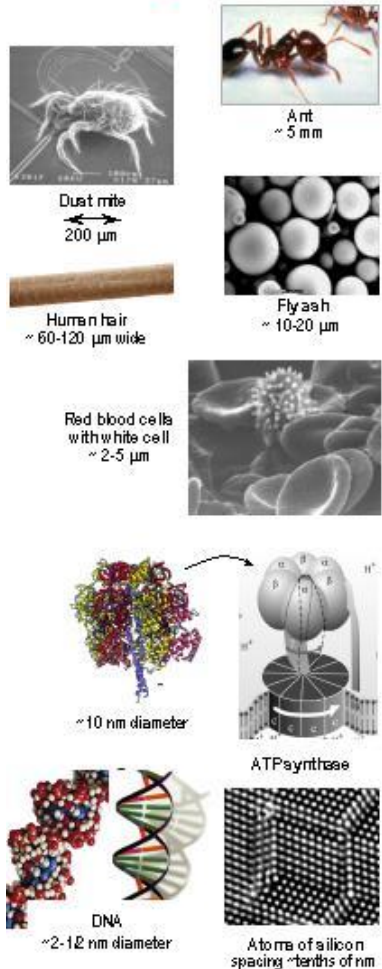
Near future

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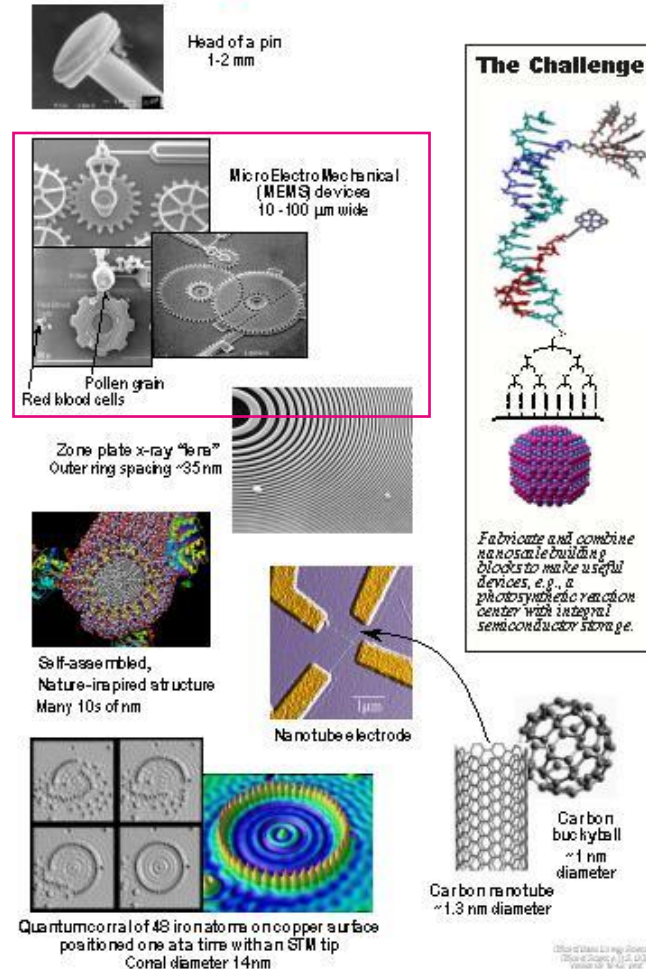
MINIATURIZATION AND SCALING

The Scale of Things – Nanometers and More

Things Natural



Things Manmade



During the 3rd industrial revolution...

Miniaturization



Microelectronics



MEMS



BioMEMS

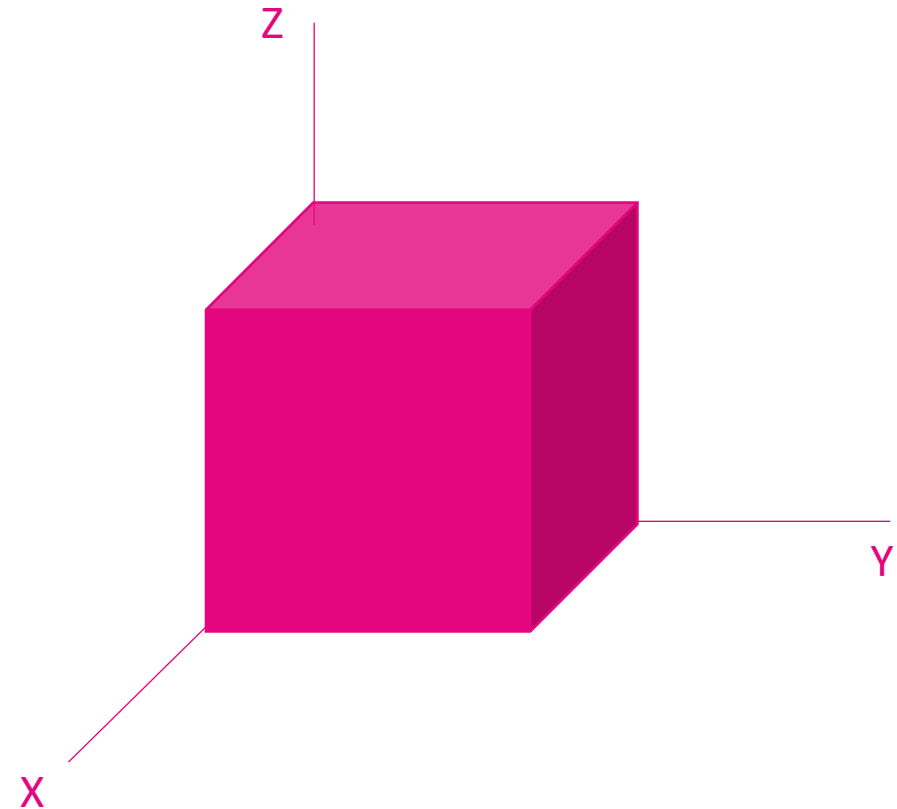
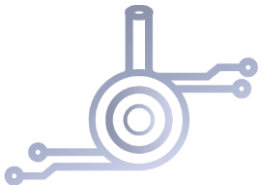


Lab-on-a-Chip

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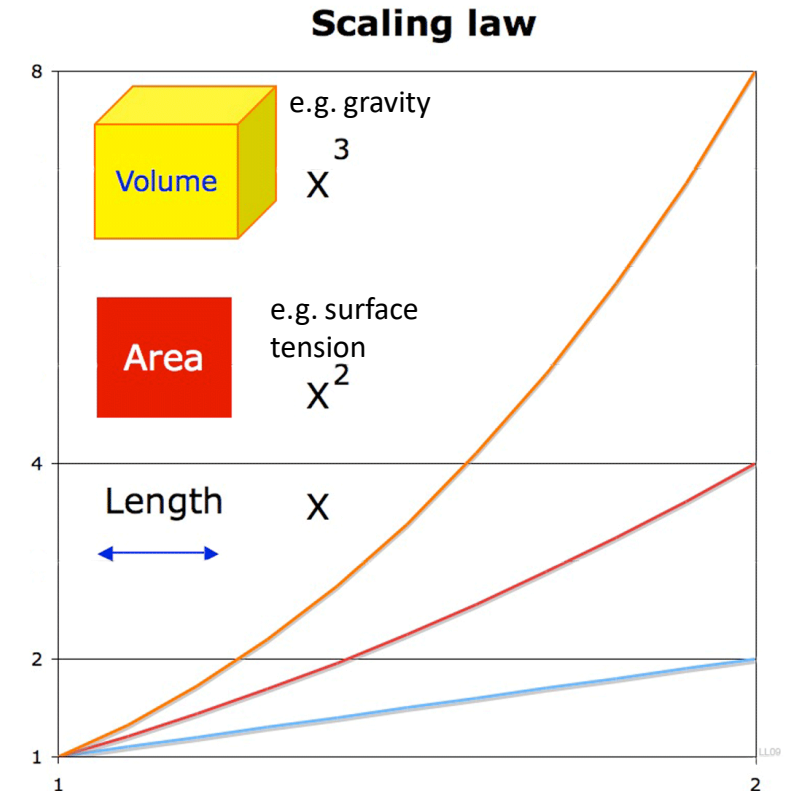
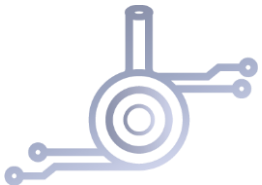
SCALING LAWS: LENGTH DIMENSION

- Length dimension: L [m]
- $Volume = L_x L_y L_z$
- Effects studied
 - Mechanical
 - Electromagnetic
 - Thermal



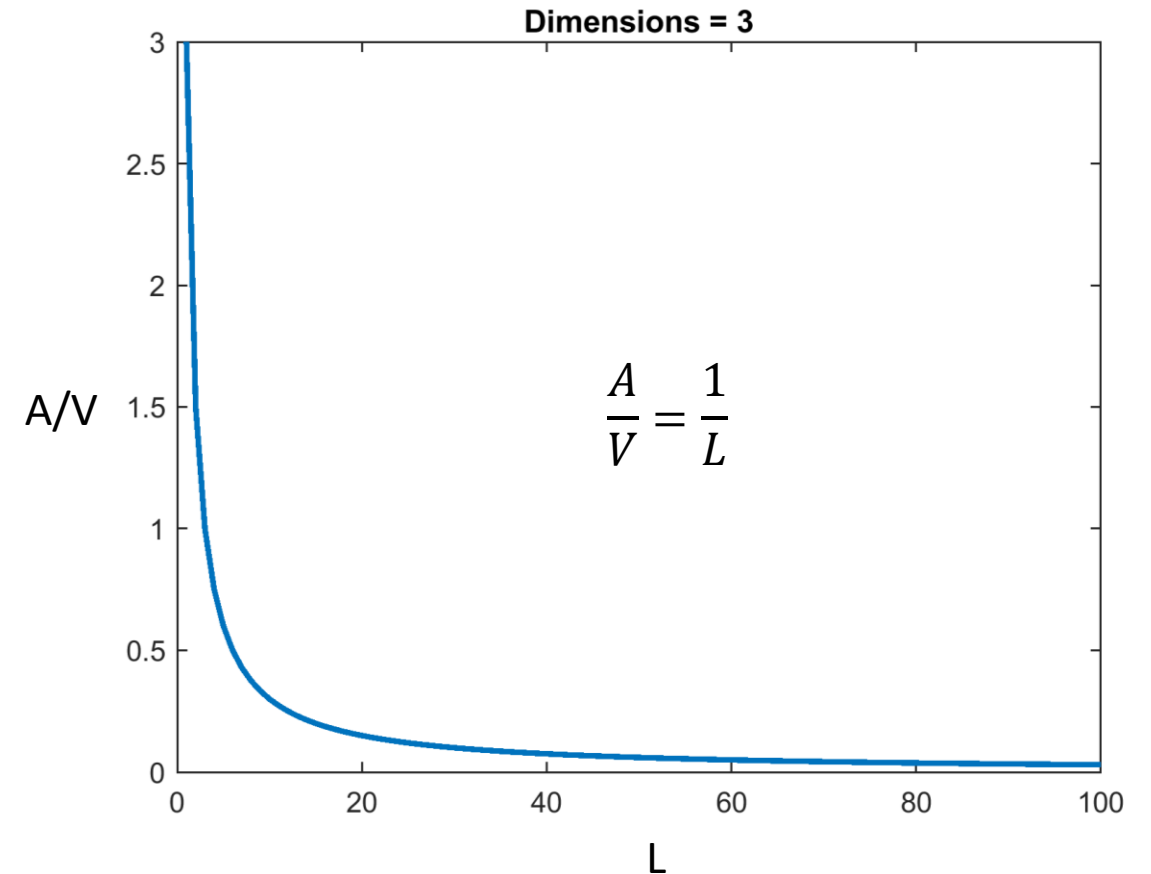
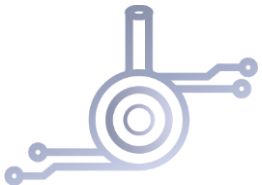
SCALING LAWS

- Scaling-down can cause unforeseen effects...
laws are the same, but they "are enforced with different strength" 😊
- Note: fluid = liquid / gas
- Microscale fluidics:
 - Gravity is negligible** compared to surface tension, friction (fluidic resistance)
 - Co-flowing fluids don't mix** apart from diffusion through interfaces



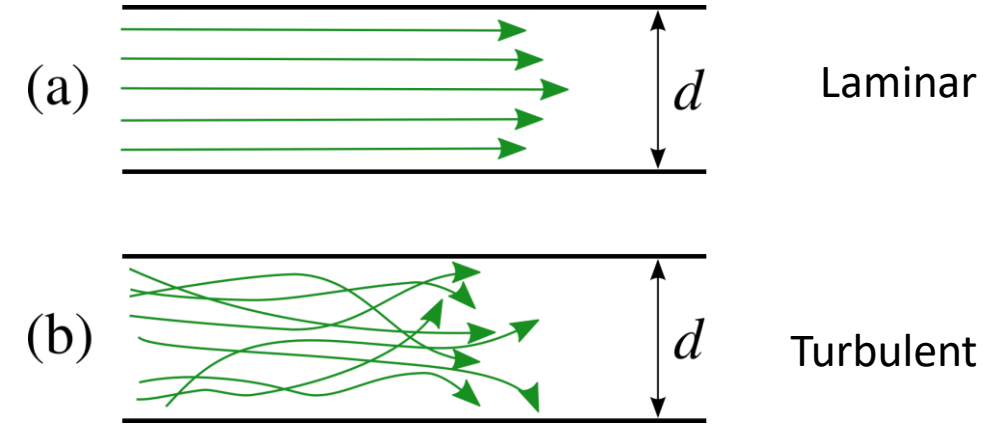
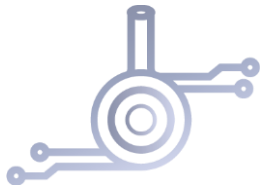
SURFACE AREA TO VOLUME RATIO (SAV)

- *Volume:* $V = L_x \cdot L_y \cdot L_z = L^3$
- *Surface:* $A = L^2$;
- **Microscale: high SAV**
 - (+) At microscale, surface tension dominates, inertial and body forces less prominent → droplet microfluidics
 - (-) surface adsorption increases → clogging

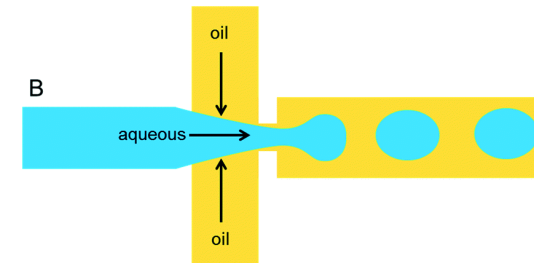
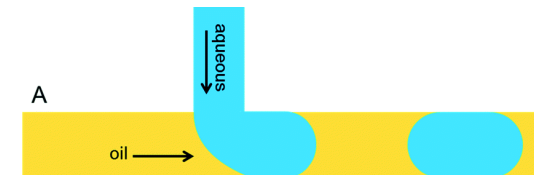


SCALING FLOWS

- Macroscale: Laminar, turbulent
- **Microscale: Laminar**
- **Time-dependence**
(based on whether/how flow depth changes in time):
steady/unsteady, whether flow depth changes over time
- **Space-dependence**
(based on whether/how flow depth changes in space):
uniform, varied, continuous, spatially varied
(discontinuous)



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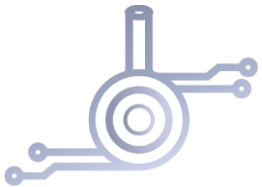


Discrete
Discontinuous
Multi-phase

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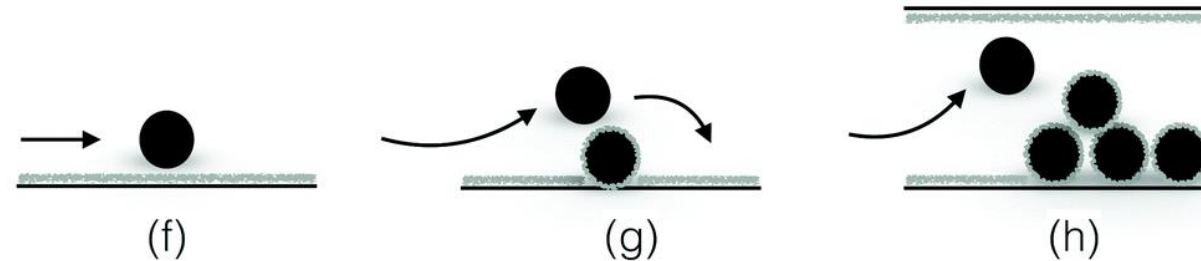
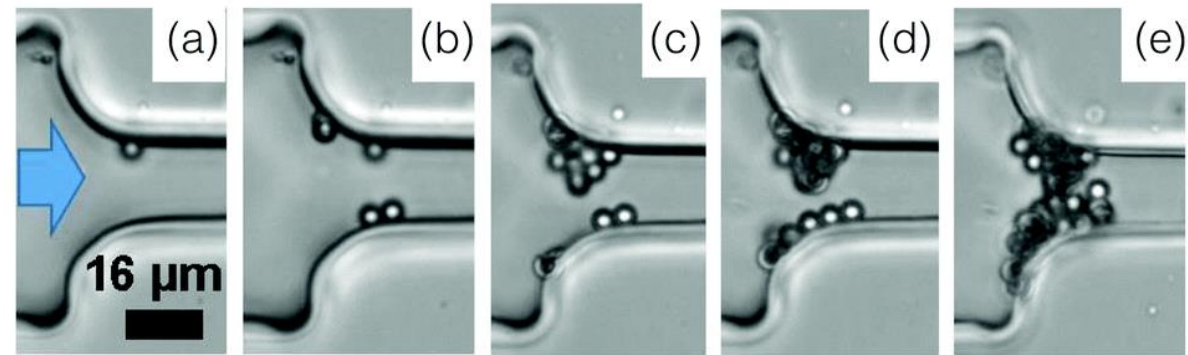
SCALING OF LAWS

- Speed: $v = \frac{s}{t}$
 - Scaling v : $v \sim L$
 - Acceleration: $a = \frac{s}{t^2}$
 - Scaling a : $a \sim L^{-1}$
 - Force: $F = m \cdot a$
 - Scaling F : $F \sim L^2$
- **10x reduction of $L \rightarrow 100x$ reduction of F**
(thus body forces are largely irrelevant in microfluidics)

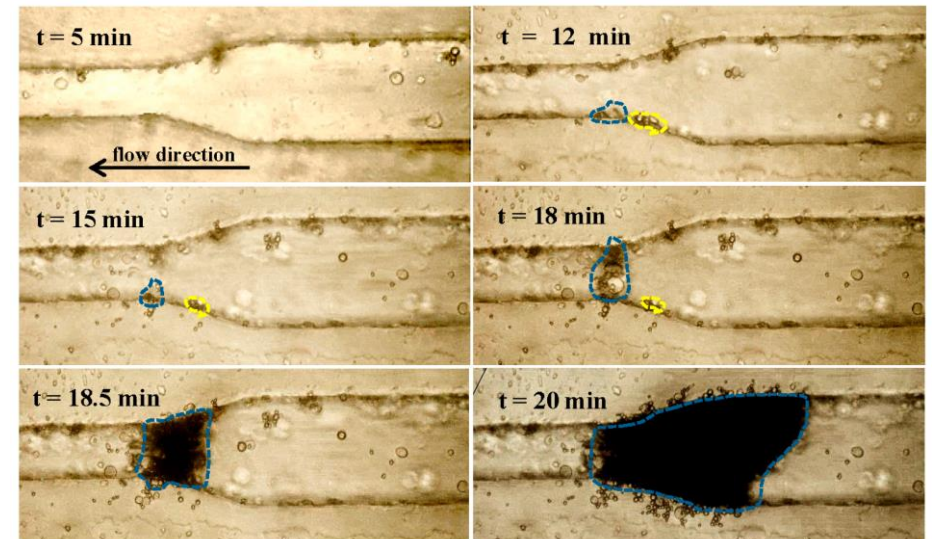


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<https://www.mdpi.com/1424-8220/17/1/106/htm>

SCALING OF LAWS

Property	Scaling factor
Velocity	$\sim L$
Time	1
Inertia	$\sim L^3$
Pressure	$\sim L$
Gravity	$\sim L^3$
Hydrostatic resistance	$\sim L^{-4}$
Capillary rise, diffusion constant	$\sim L^{-1}$

- Inertial forces and gravity $\sim L^3$
 - If inertial force scales relative to characteristic length L by a factor of L^3 then if length decreases 10 times, force decreases 1000 times
 - Similarly, the effect of gravity decreases 1000 times ($1/1000^{\text{th}}$ if length is $1/10^{\text{th}}$)
 - Thus, the effects of body forces and gravity are minimal on the microscale
- Viscoelastic forces $\sim L^{-4}$
 - However, the effect of viscoelastic forces is significantly amplified (for a length of $1/10^{\text{th}}$, 10000 times)



SCALING LAWS

- Context
- Scaling of forces
- Effect of forces on microscale flows

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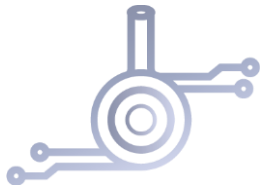
BASIC FLUID MECHANICS

- Continuum assumption
- Newtonian and non-newtonian fluids
- Flow types
- Diffusion
- Surface tension
- Contact angle

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FLUID MECHANICS

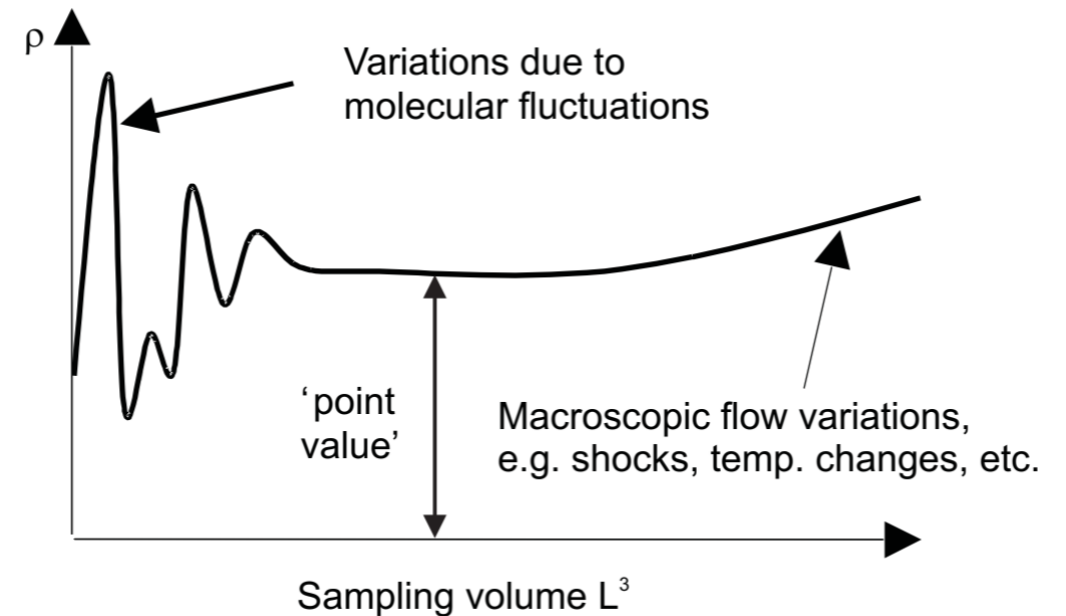
- Dominant properties of fluid flow:
 - **Kinematic**
(angular velocity, acceleration etc.)
 - **Transport**
(viscosity, thermal conductivity, diffusivity)
 - **Thermodynamic**
(pressure, temperature, density)
 - **Miscellaneous**
(surface tension, etc.)



Continuum assumption is valid on macroscale and mostly valid on microscale (NB! effect of intermolecular forces becomes dominant as we downscale)

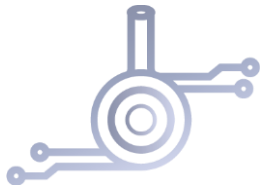
Continuum assumption:

properties are defined everywhere in space and vary continuously over the flow between two points



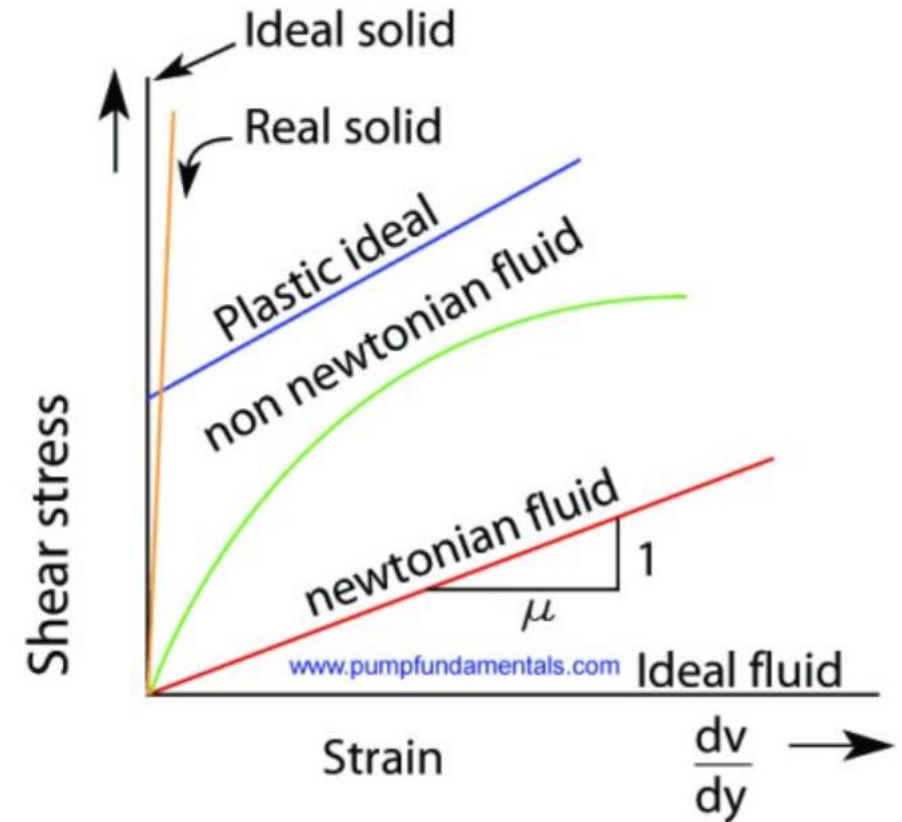
BASIC PROPERTIES OF FLUIDS

- **Newtonian fluid: constant viscosity**
 - Viscosity remains constant, irrespective of shear stress applied at constant temperature (viscosity-shear stress relation linear)
- **Non-Newtonian: non-constant viscosity**
 - Time-independent viscosity (e.g. ketchup, grease)
 - Time dependent as function of deformation and time history (e.g. yoghurt)
 - Viscoelastic: able to recover part of deformation energy (e.g. lubricants)



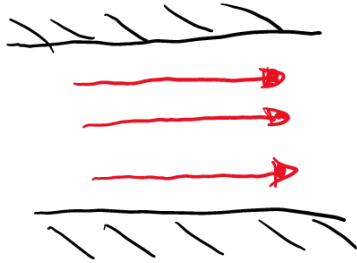
Stress: force over area

Strain: change in length / original length



https://www.pumpfundamentals.com/pump_glossary.htm

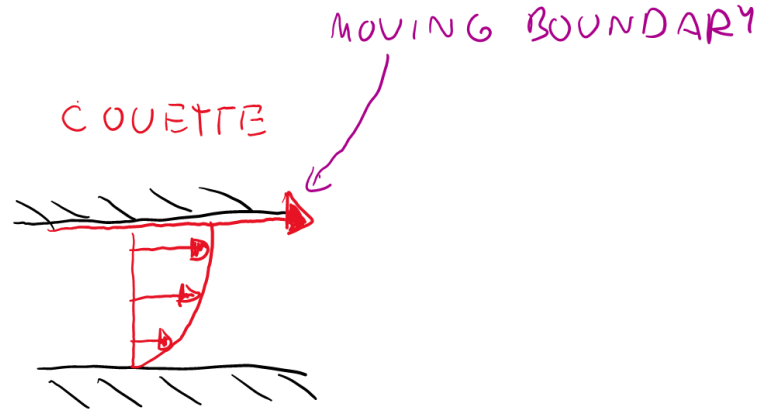
FLOW TYPES



UNIFORM
FLOW

~ ELECTROOSMOTIC

[Uniform Flow | Fluid Mechanics - YouTube](#)



SHEAR
FLOW

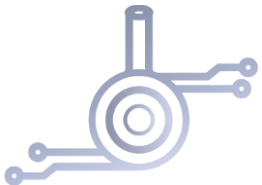
RELATIVE
MOTION BETWEEN
BOUNDARIES



PARABOLIC
FLOW

PRESSURE -DRIVEN
FLOW

[Viscosity and Poiseuille flow | Fluids |
Physics | Khan Academy - YouTube](#)



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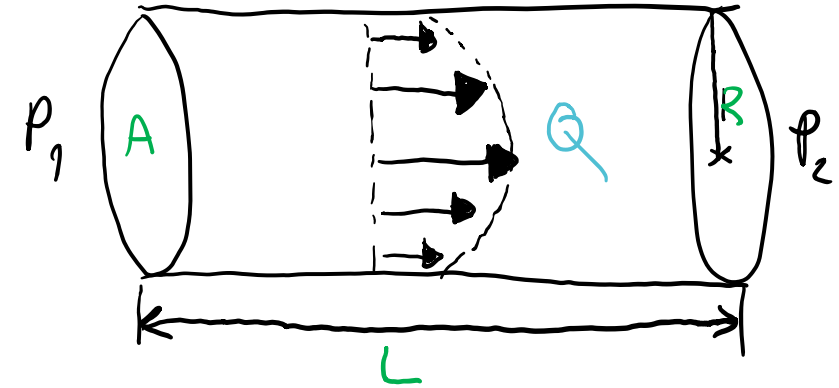
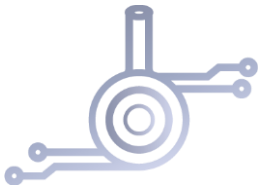
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HAGEN-POISEUILLE EQUATION

- Parabolic flow profile:
 - Flow is pressure-driven
 - No-slip boundary condition applies (boundary is solid, flow velocity zero at boundary)

$$\Delta p = \frac{8\pi\mu L Q}{A^2} = \frac{8\mu L Q}{\pi R^4}$$

- Pressure-driven flow types:
 - Negative pressure (e.g. vacuum at outlet)
 - Positive pressure (e.g. pump on inlet)



μ : dynamic viscosity [Pa · s]

p : pressure [Pa]

A : pipe cross section [m²]

R : pipe radius [m]

Q : flow rate $\left[\frac{\text{m}^3}{\text{s}}\right]$

DIFFUSION

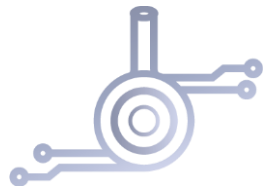
- Estimation of diffusion length:

$$L_D = \sqrt{4Dt} = 2\sqrt{Dt}$$

- Estimation of diffusion coefficient

$$\frac{D_{T_1}}{D_{T_2}} = \frac{T_1}{T_2} \frac{\mu_{T_2}}{\mu_{T_1}}$$

- What's the point of all this? In microfluidics, mixing mostly happens by diffusion, through the fluid interfaces



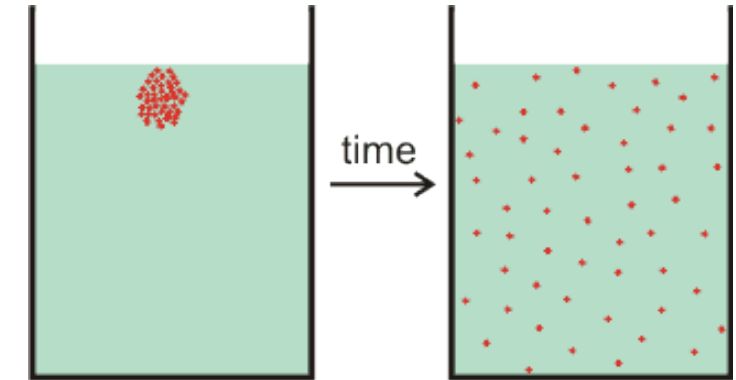
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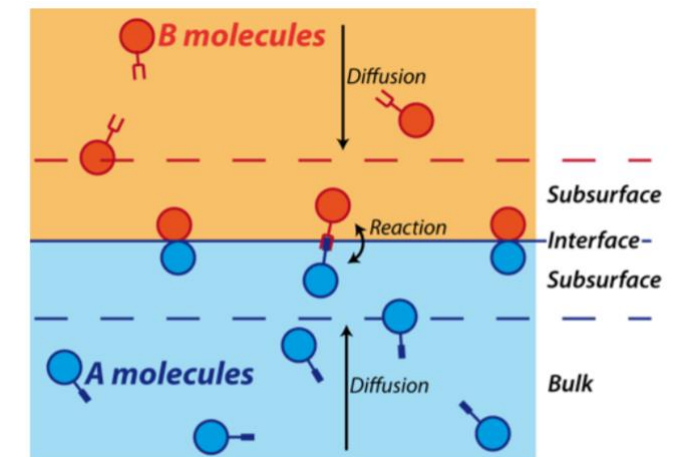
μ : dynamic viscosity [Pa · s]

T : temperature [K]

D : diffusion coefficient $\left[\frac{m^2}{s}\right]$



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<https://arxiv.org/pdf/1708.02804.pdf>

INTERFACES AND SURFACE TENSION

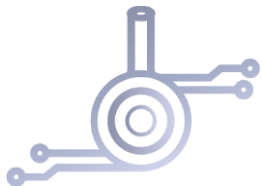
- **Van der Waals attraction**

- *In organic liquids, hydrogen bonds in polar liquids hold molecules close to each other*
- *However, at an interface, half of the interactions are with molecules from the other phase (gas/liquid)*
- *On a macroscopic level, this results in a clear interface (there's "tension between the surfaces of the two phases")*

- Surface tension:

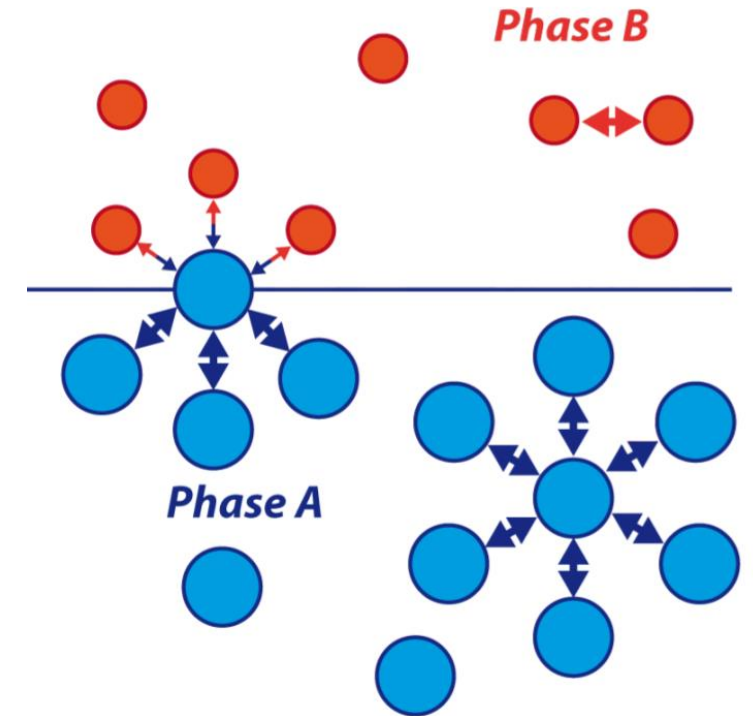
$$\gamma \approx \frac{U}{2\delta^2} \left[\frac{J}{m^2} \right]$$

Where U: total cohesive energy per molecule [J], δ characteristic molecular dimension (δ^2 area of same [m^2])

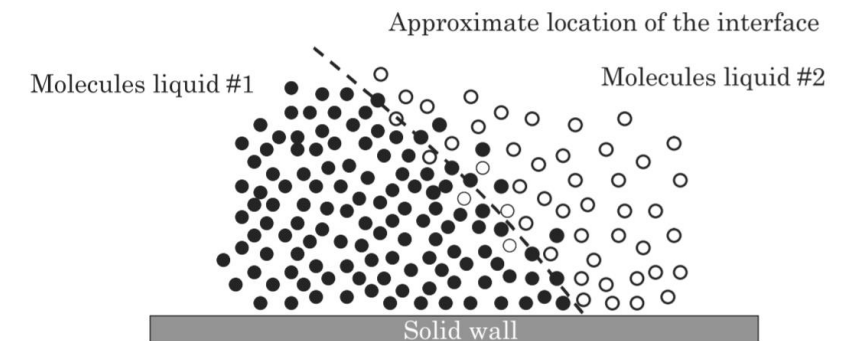


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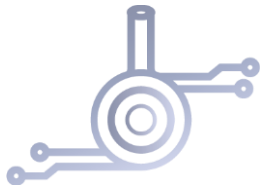
INTERFACES AND SURFACE TENSION

- Van der Waals attraction

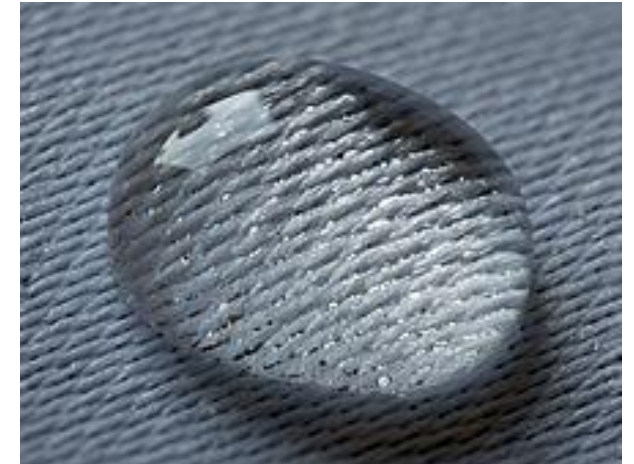
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- However, at an interface, half of the interactions are with molecules from the other phase (gas/liquid)
- On a macroscopic level, this results in a clear interface (there's "tension between the surfaces of the two phases")

- **Surface tension:**

$$\gamma \approx \frac{U}{2\delta^2} \left[\frac{J}{m^2} \right]$$



Where U: total cohesive energy per molecule [J], δ characteristic molecular dimension (δ^2 area of same [m^2])



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INTERFACES AND SURFACE TENSION

- **Surface tension:**

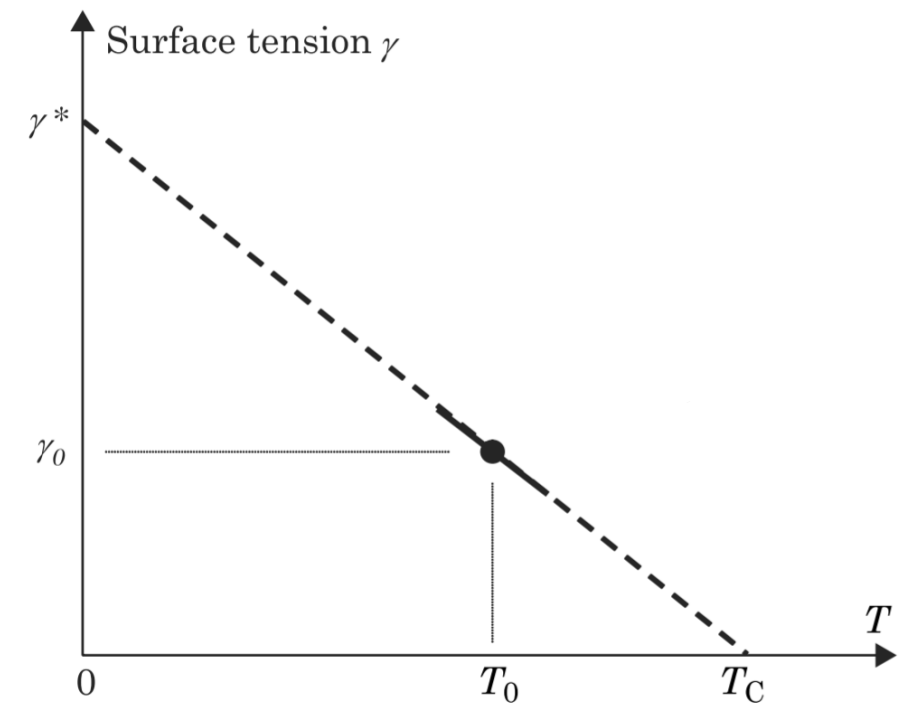
$$\gamma \approx \frac{U}{2\delta^2} = \frac{\Delta E_f}{\Delta A} \left[\frac{J}{m^2} \right]$$

Where U: total cohesive energy per molecule [J], δ characteristic molecular dimension (δ^2 area of same [m^2])
Aka. the E_f surface energy [J] required to maintain surface area A [m^2].

- **Temperature dependence**

$$\gamma_0 = \gamma^* \frac{T_C - T_0}{T_C}$$

- Where: γ_0 : reference surface tension (in air at 20 °C)



Liquid	γ_0
Water	72.8
Mercury	425.4
Ethanol	22.1
Glycerol	64.0
PDMS	19.0

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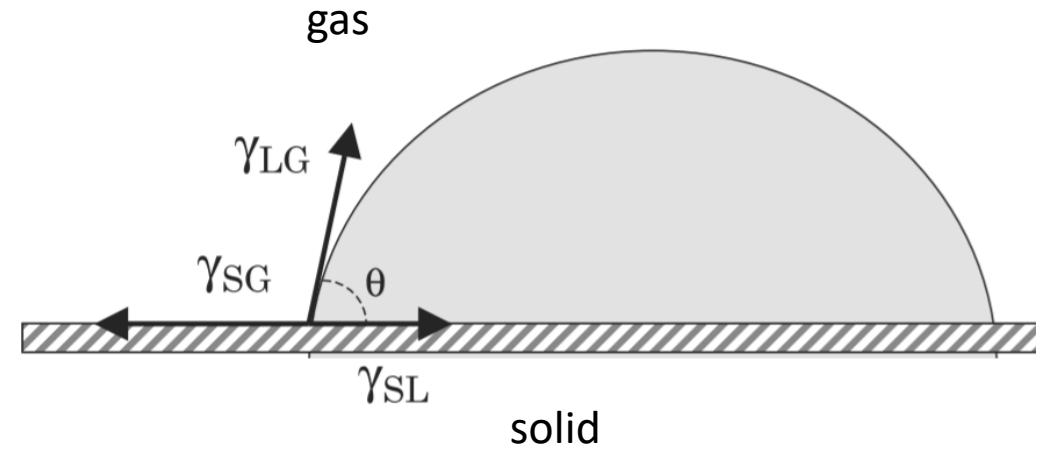
CONTACT ANGLE AND WETTING

$$\gamma_{LG} \cdot \cos\theta = \gamma_{SG} - \gamma_{SL}$$

$$\theta = \arccos \frac{\gamma_{SG} - \gamma_{SL}}{\gamma_{LG}}$$

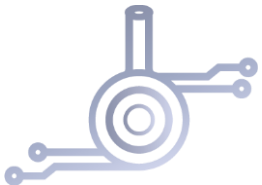
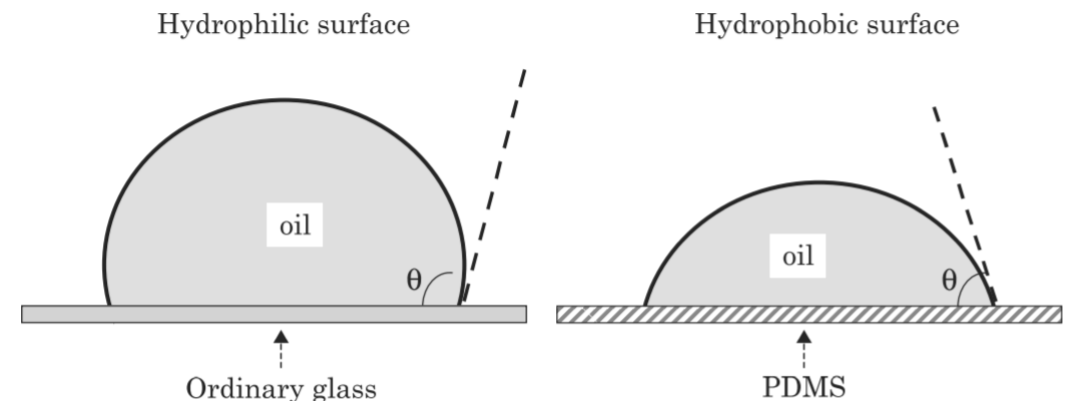
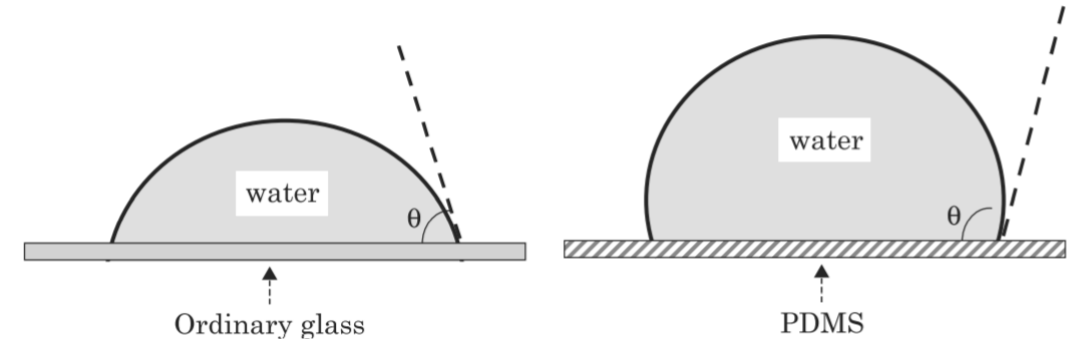
■ Triple contact line

- Between solid, gas and liquid, surface tensions at equilibrium are related as on the right
- The contact angle that the liquid interface closes with the solid surface, is denoted θ



Hydrophilic contact $\theta < 90^\circ$

Hydrophobic contact $\theta > 90^\circ$



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CAPILLARY AND HYDROSTATIC PRESSURE

- Capillary pressure in a tube:

$$\Delta p = \frac{2\gamma}{R}$$

- Capillary rise in a tube:

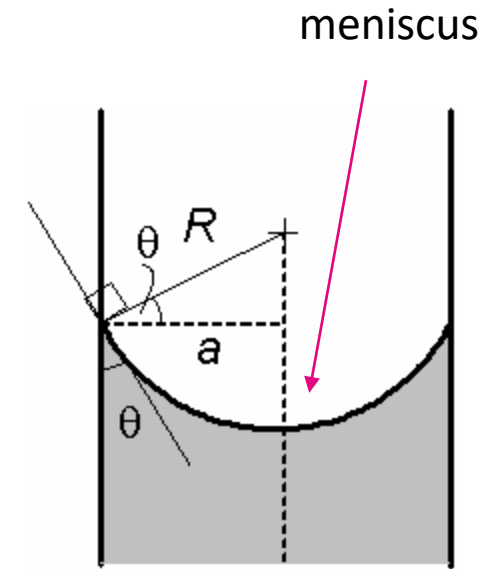
$$h = \frac{2\gamma \cos \theta}{\rho g a}$$

- Hydrostatic pressure
 $p = \rho g h$

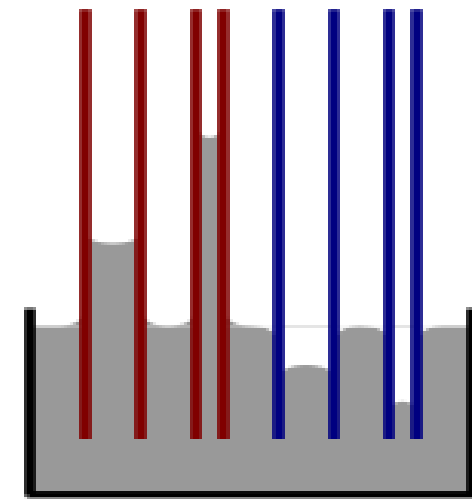
h: height/depth of fluid column [m]

p : pressure [Pa]

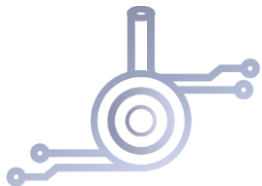
ρ : density $\left[\frac{\text{kg}}{\text{m}^3} \right]$



https://upload.wikimedia.org/wikipedia/commons/7/75/Spherical_meniscus.PNG



<https://upload.wikimedia.org/wikipedia/commons/thumb/8/85/CapillaryAction.svg/270px-CapillaryAction.svg.png>



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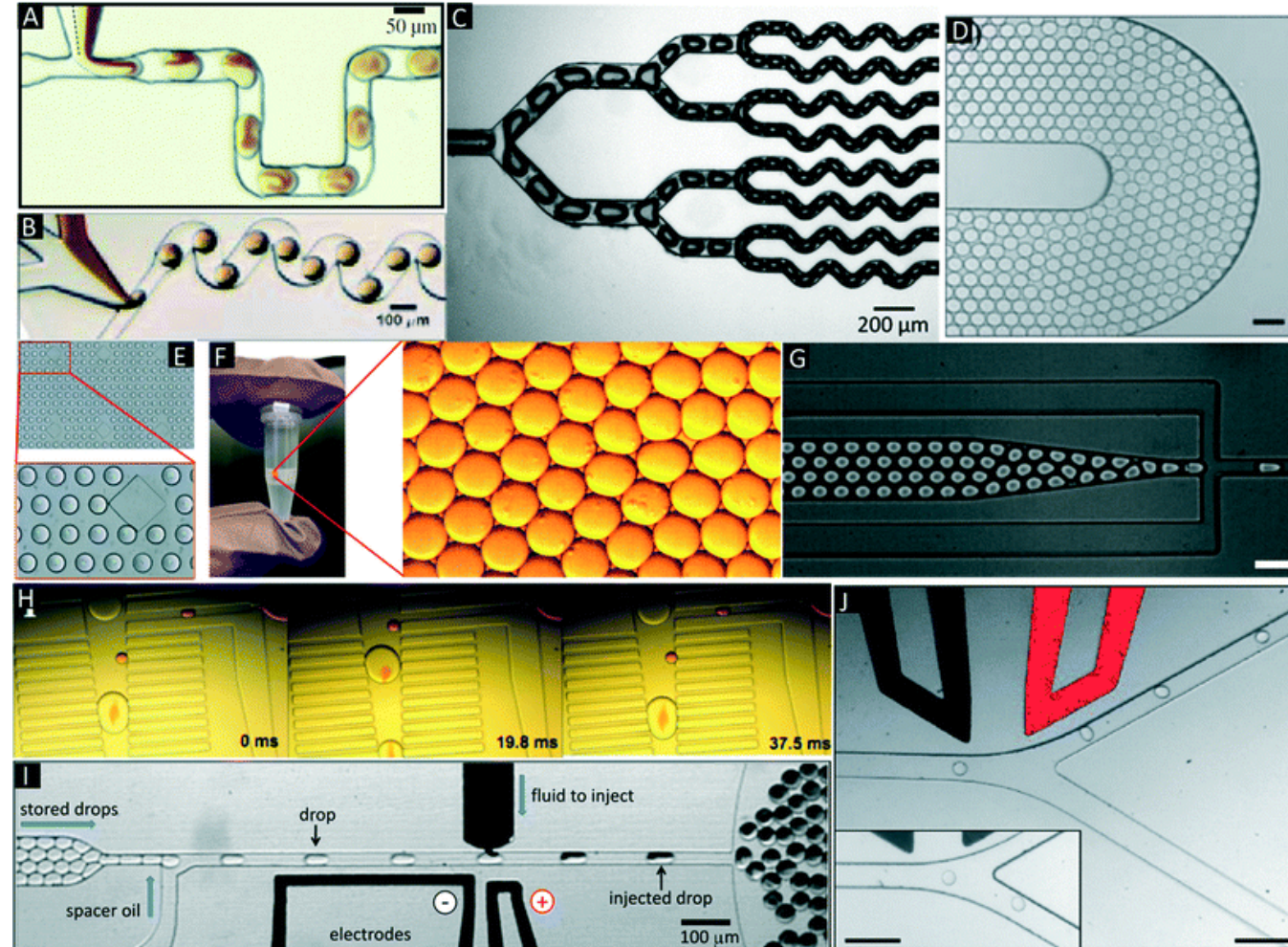
INTRODUCTION TO DROPLETS

- Young's law
- Laplace law
- Capillary pressure
- Surfactants

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INTRODUCTION

- (+) Excellent **volume control**
- (+) **Chemical separation** between droplets
- (+) Ability to implement packed bed microreactors
- (+) **Storage** of droplets
- (-) Technologically challenging
 - Monodispersity
 - Generation rate
 - Droplet stability
 - Minimum droplet volume



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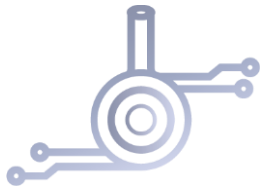
YOUNG'S LAW

- Young's law:
The contact angle that the liquid interface closes with the solid surface, is denoted θ

$$\gamma_{LG} \cdot \cos\theta = \gamma_{SG} - \gamma_{SL}$$

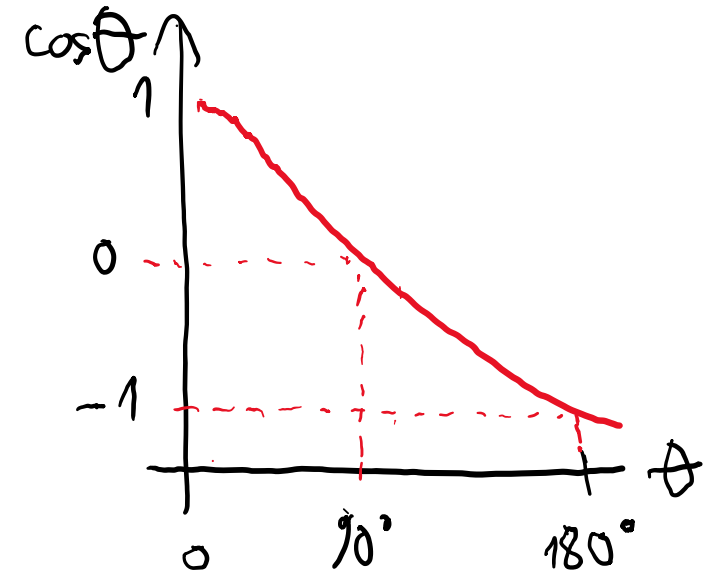
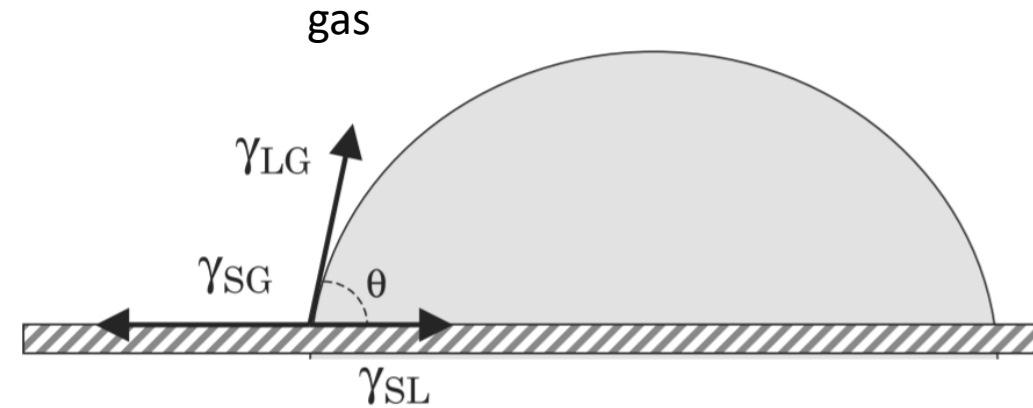
- Work of adhesion:

$$W_a = \gamma + \gamma_{SG} - \gamma_{SL} = \gamma(1 + \cos\theta)$$



Superhydrophobic: $\cos\theta \rightarrow -1$; $W_a \rightarrow 0$

Superhydrophilic: $\cos\theta \rightarrow 1$; $W_a \rightarrow \infty$



LAPLACE LAW

- Pendant drop

Starting from a pendant drop (hanging from a vertical pipe, like your tap at home)

- Laplace law for a sphere:

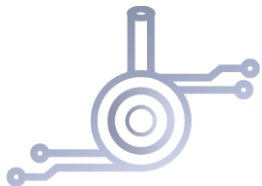
$$\Delta p = p_0 - p_1 = \frac{2\gamma}{R}$$

- Young-Laplace:

$$\Delta p = \rho g h - \gamma \left(\frac{1}{R_1} + \frac{1}{R_2} \right)$$

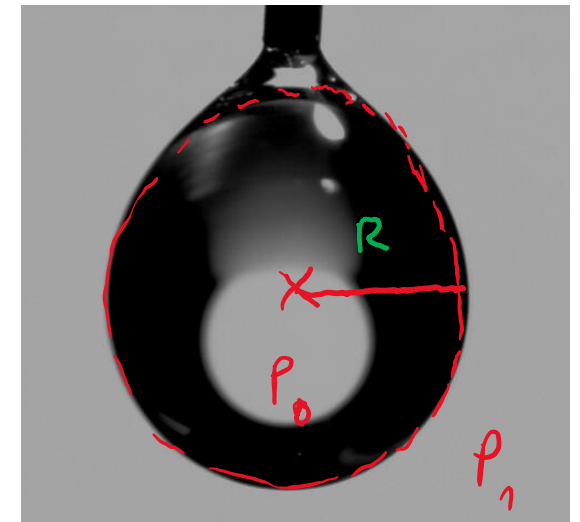
(hydrostatic pressure $\leftrightarrow$ surface tension)

(this is how surface tension can be experimentally determined)

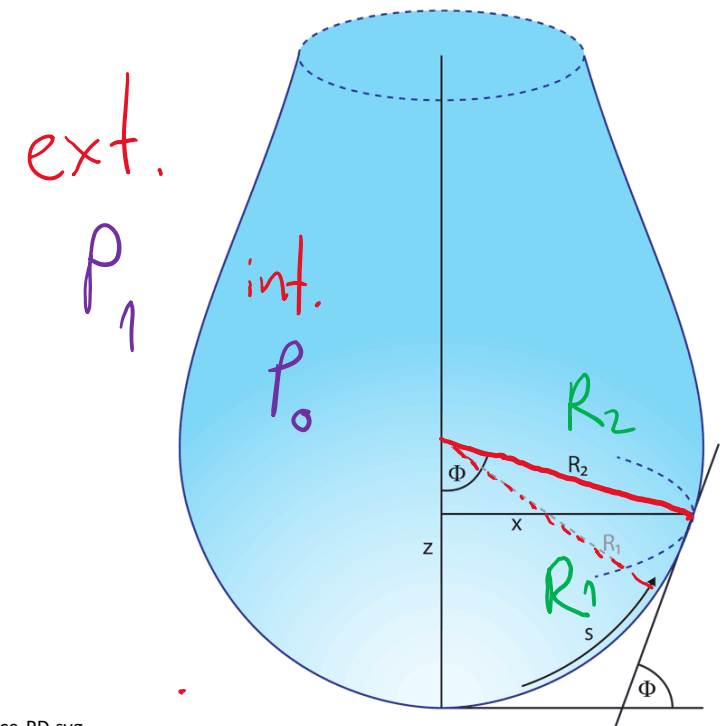


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CAPILLARY FORCE BETWEEN PARALLEL PLATES

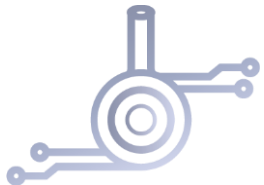
- Laplace law for the free interface:

- $R_2 \sin\left(\frac{\pi}{2} - \theta\right) = \frac{h}{2} \rightarrow R_2 = \frac{h}{2\cos\theta}$

- Laplace law: $\Delta P = \gamma\left(\frac{1}{R} - \frac{2\cos\theta}{h}\right)$

- Capillary pressure: $\Delta p \approx -\frac{2\gamma\cos\theta}{h}$

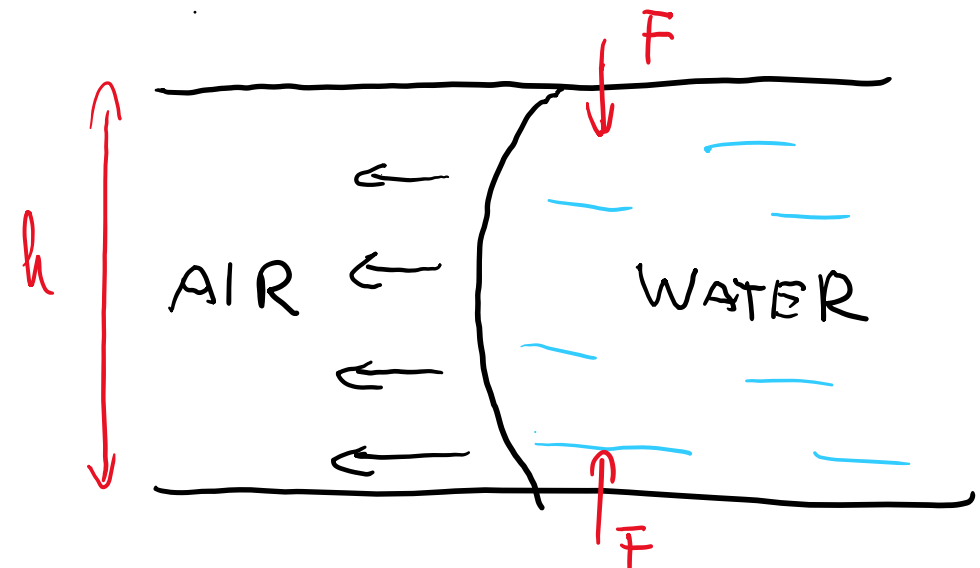
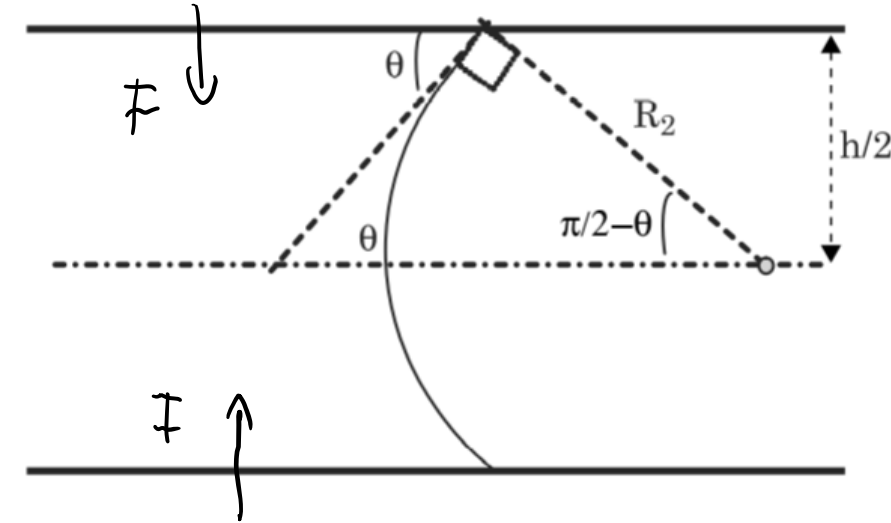
- Capillary force: $F \approx \frac{2\gamma\cos\theta}{h}\pi R^2$



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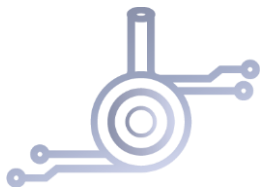
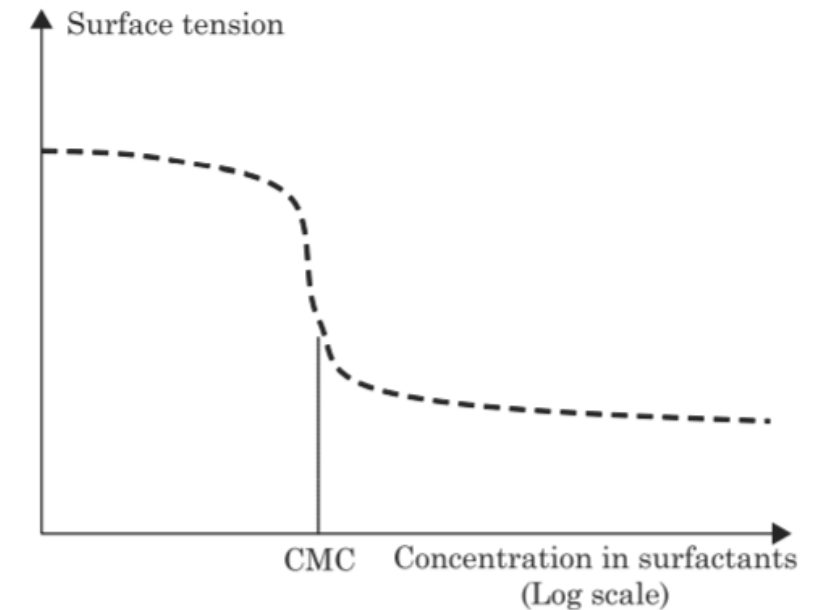
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Example:
 $h = 10\mu\text{m}, R = 1\text{cm}, F \approx 2.5\text{ N}$



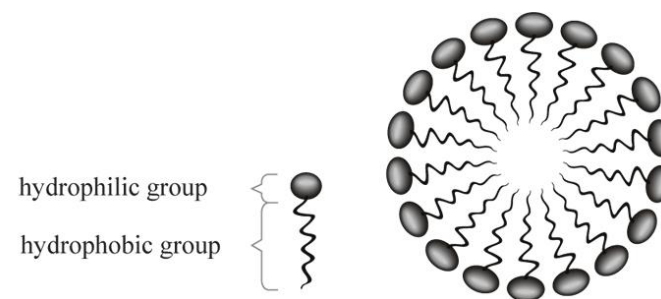
SURFACTANTS

- Surfactant = surface active agent
 - Hydrophilic head
 - Hydrophobic tail
- Surfactants decrease surface tension
 - CMC = critical micelle concentration → “stable droplets”
 - Think of soap ☺
 - Example:
 - Water surface tension 72 mN/m
 - Tween 10 + water above CMC: 30 mN/m

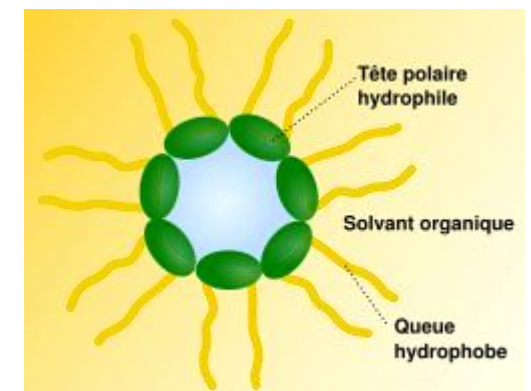


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INTRODUCTION TO DROPLETS

- Young's law
- Laplace law
- Capillary pressure
- Surfactants

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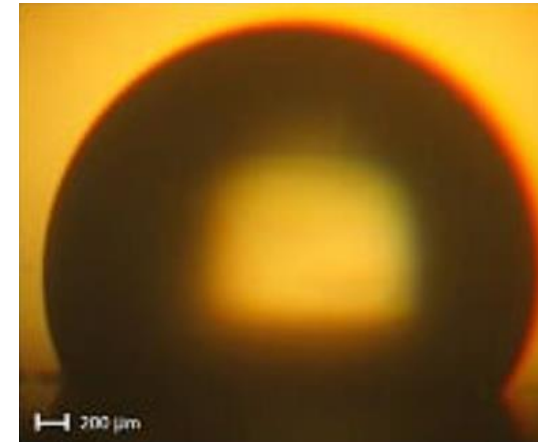
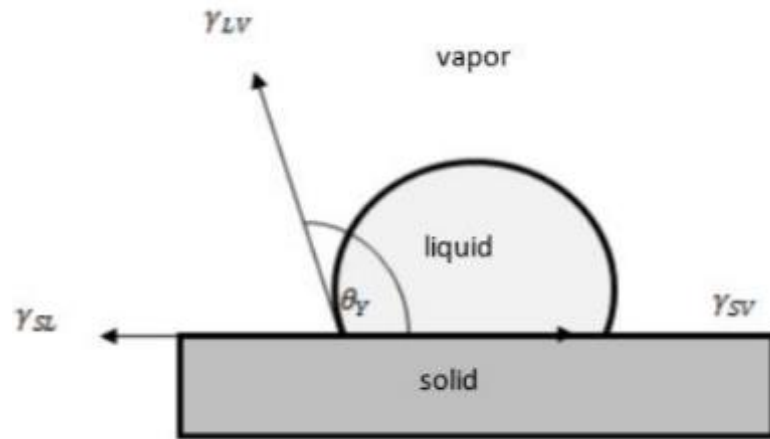


SUPERHYDROPHOBIC SURFACES

- Contact angle and wetting on micropatterned surfaces
- ...on rectangular micropillars
- ...in nature

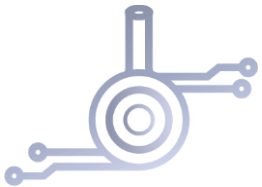
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THEORY: DROPLETS



Equilibrium contact angle

$$\cos\theta_0 = \frac{\gamma_{SV} - \gamma_{SL}}{\gamma_{LV}}$$



DROPLETS ON MICROPATTERNED SURFACES

- **Roughness factor - micropatterned surface:**

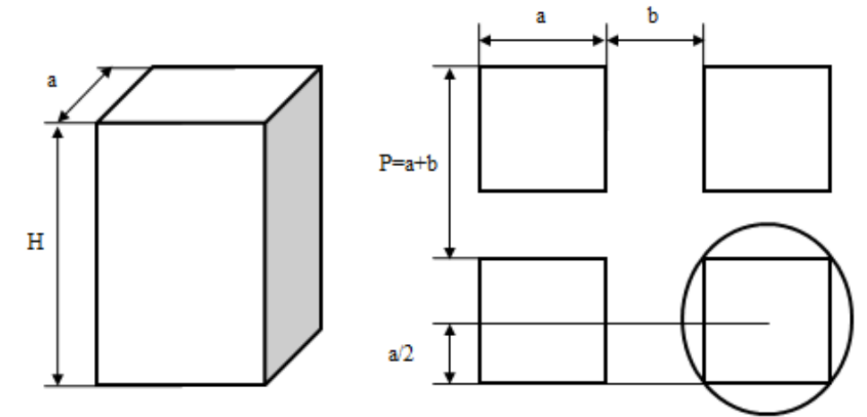
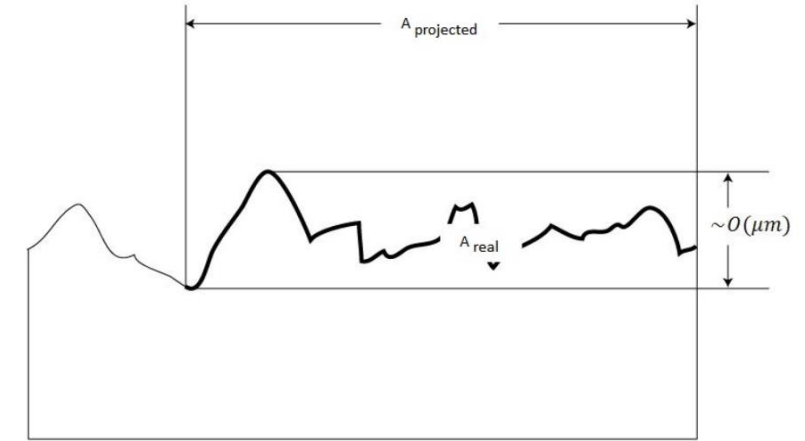
$$r = \frac{A_{real}}{A_{projected}}$$

- For rectangular micropillars:
 - Roughness factor - homogeneous interface:

$$r = \frac{(a + b)^2 + 4aH}{(a + b)^2}$$

- Roughness factor - inhomogeneous interface:

$$f = \frac{A_{top}}{A_{projected}} = \frac{a^2}{(a + b)^2} = A$$



DROPLETS ON MICROPATTERNED SURFACES

- Roughness factor - micropatterned surface:

$$r = \frac{A_{real}}{A_{projected}}$$

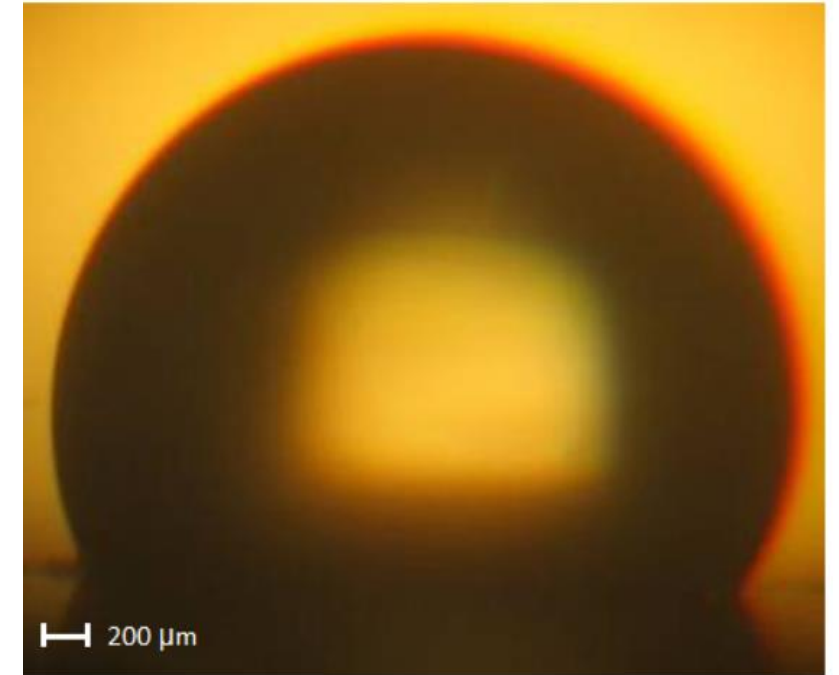
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- Roughness factor - inhomogeneous interface:

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Wenzel state



Contact angle: $\cos\theta_W = r\cos\theta_0$

On rectangular micropillars:

$$\cos\theta_W = \left[1 + \frac{4A}{\left(\frac{a}{H}\right)}\right] \cdot \cos\theta$$

DROPLETS ON MICROPATTERNED SURFACES

- Roughness factor - micropatterned surface:

$$r = \frac{A_{real}}{A_{projected}}$$

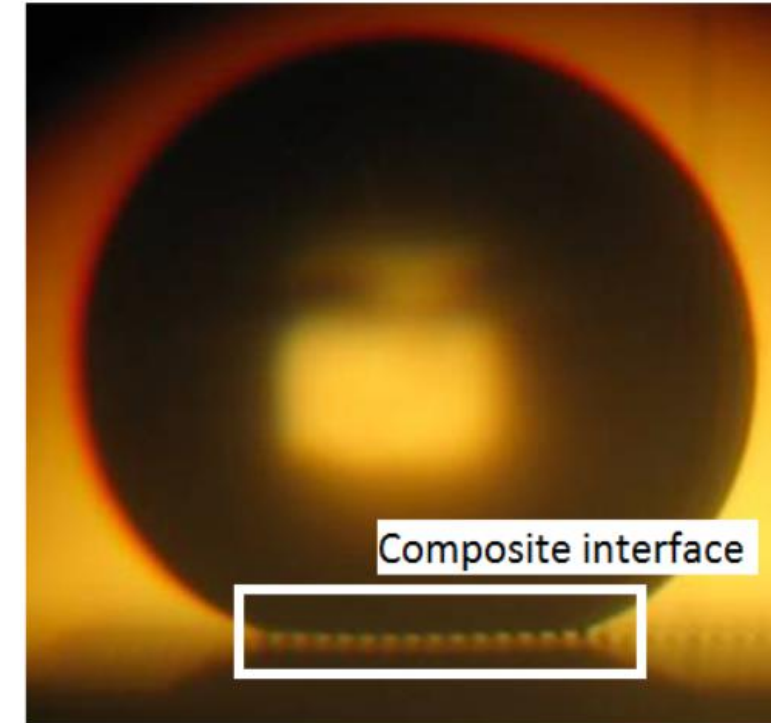
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- **Roughness factor - inhomogeneous interface**:

$$f = \frac{A_{top}}{A_{projected}} = \frac{a^2}{(a + b)^2} = A$$

Cassie state



Contact angle: $\cos\theta_c = f_1\cos\theta_1 + f_2\cos\theta_2$

On rectangular micropillars:

$$\cos\theta_c = -1 + A(1 + \cos\theta)$$

DROPLETS ON MICROPATTERNED SURFACES

- Roughness factor - micropatterned surface:

$$r = \frac{A_{real}}{A_{projected}}$$

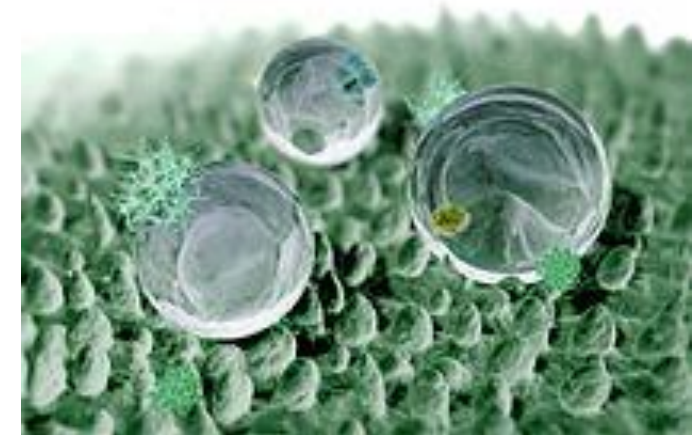
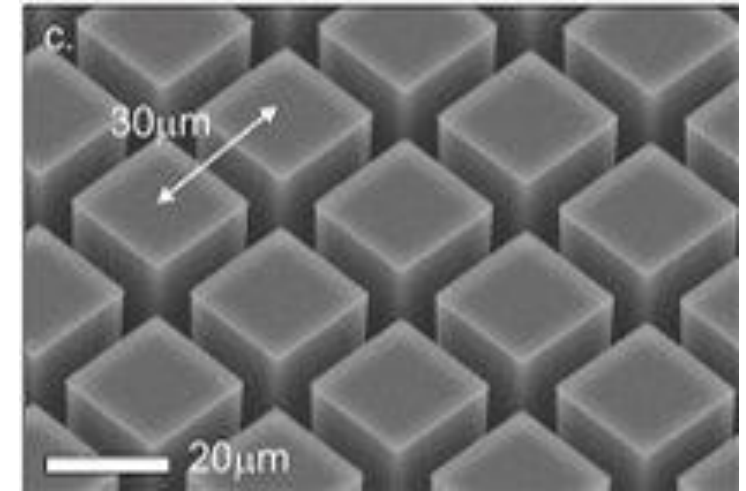
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Cassie state



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DROPLETS ON MICROPATTERNED SURFACES

Cassie state

- Roughness factor - micropatterned surface:

$$r = \frac{A_{real}}{A_{projected}}$$

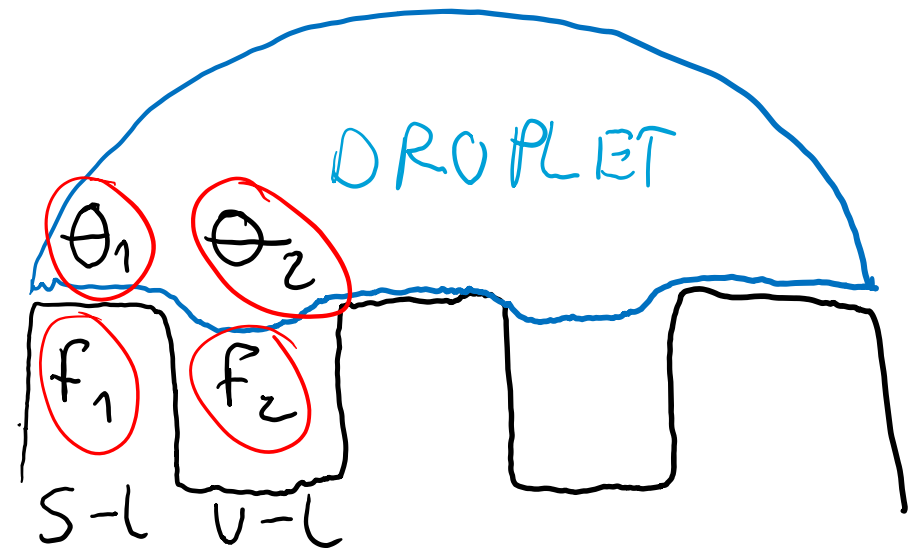
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DROPLETS ON MICROPATTERNED SURFACES

- Roughness factor - micropatterned surface:

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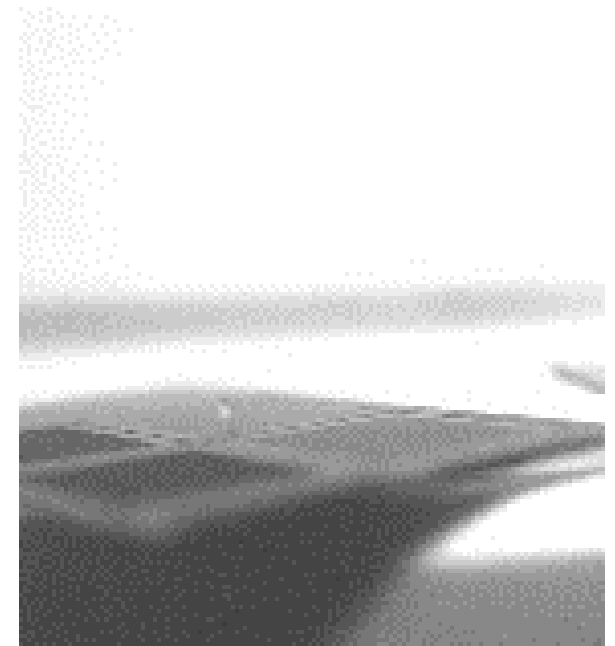
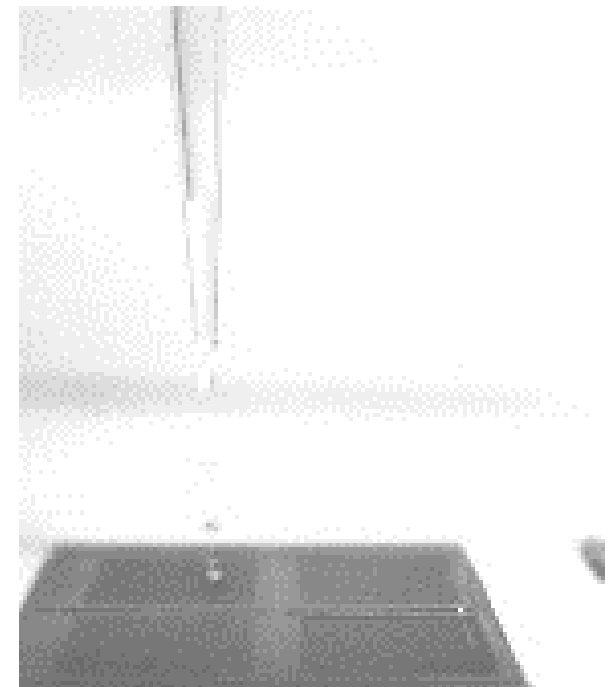
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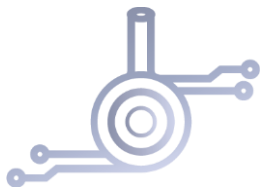
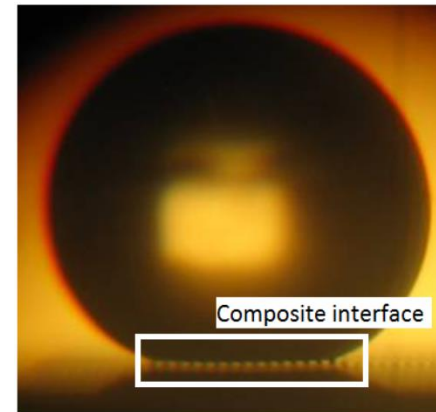
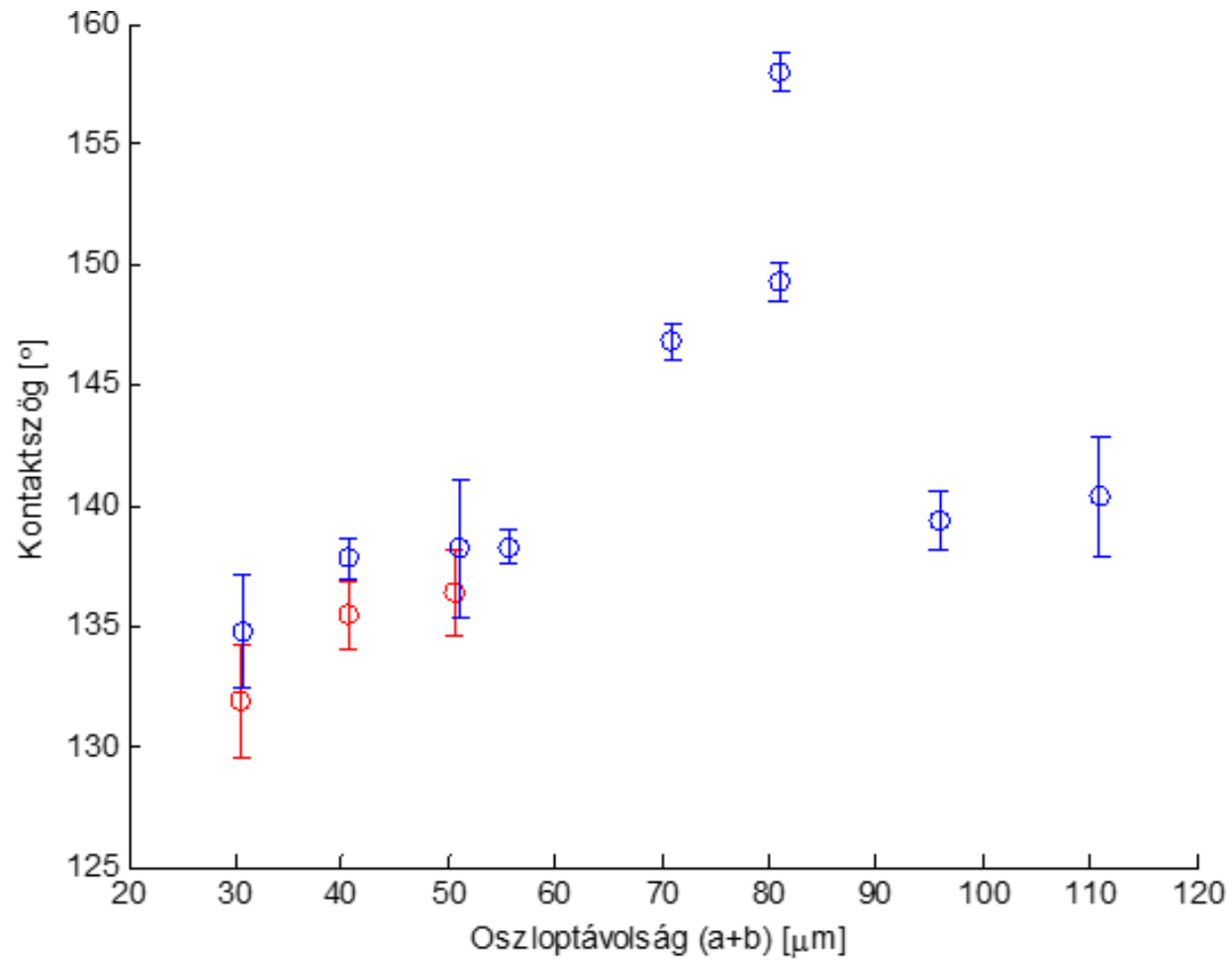
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- **Roughness factor - inhomogeneous interface**:

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CONTACT ANGLE AND WETTING





SUPERHYDROPHOBIC SURFACES

- Contact angle and wetting on micropatterned surfaces
- ...on rectangular micropillars
- ...in nature

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PRESSURE AND FLOW RATE IN MICROCHANNELS

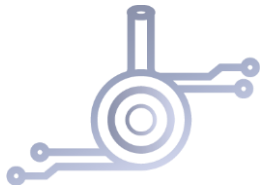
- Poisson equation
- Application to channels with...
- ...circular cross section
- ...rectangular cross section
- Flow control in microfluidics

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POISSON EQUATION

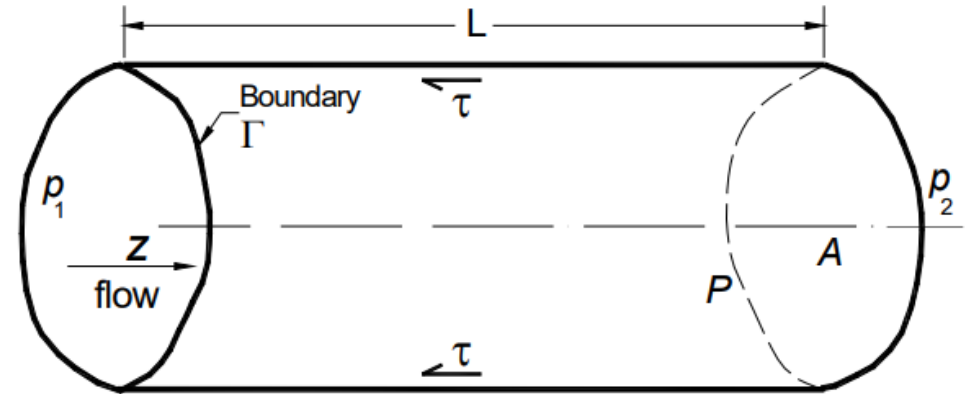
$$\nabla^2 w = \frac{1}{\mu} \frac{dp}{dz}$$

- Assuming
 - Constant velocity profile in longitudinal direction
 - Fully-developed laminar flow
 - Zero flow velocity on Γ boundary ($w = 0$ on Γ)



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w : flow velocity $\left[\frac{m}{s}\right]$

p : pressure [Pa]

μ : dynamic viscosity [Pa · s]

Γ : boundary of duct (tube)

z : flow direction

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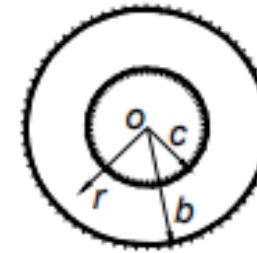
CIRCULAR MICROCHANNEL

- Analytical solution exists for mean velocity $\bar{w}$ in:
 - Circular microchannel
 - Laminar flow

$$\bar{w} = \frac{\Delta p b^2}{8\mu L} \left(\epsilon^2 - 1 + \frac{2 \ln\left(\frac{1}{\epsilon}\right) + \epsilon^2 - 1}{\ln\left(\frac{1}{\epsilon}\right)} \right)$$

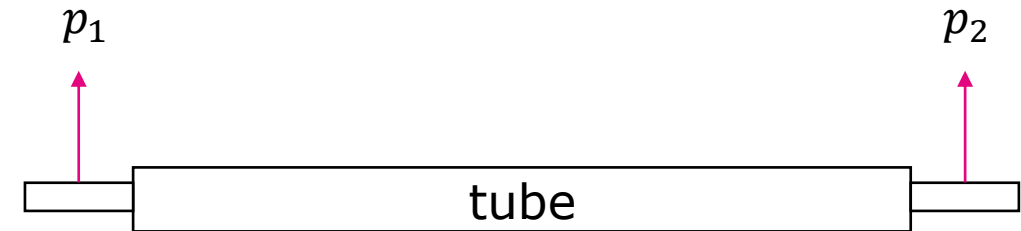
- Values:

- Semi-axes b (major), c (minor), $b \geq c$
- Δp pressure drop; $p_1 - p_2$ ($p_1 \geq p_2$)
- L : channel length [m]
- ϵ : aspect ratio; $\epsilon = \frac{c}{b}$



$$A = \pi (b^2 - c^2)$$

$$P = 2\pi (b + c)$$



w : flow velocity $\left[\frac{m}{s}\right]$

p : pressure [Pa]

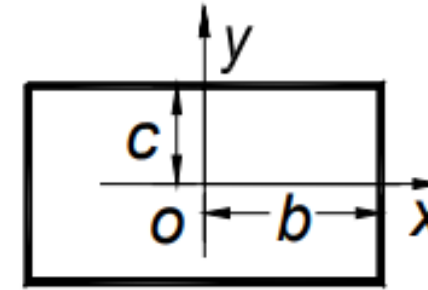
μ : dynamic viscosity [Pa · s]

RECTANGULAR MICROCHANNEL

- Analytical solution exists for mean velocity $\bar{w}$ in:
 - Rectangular microchannel
 - Laminar flow

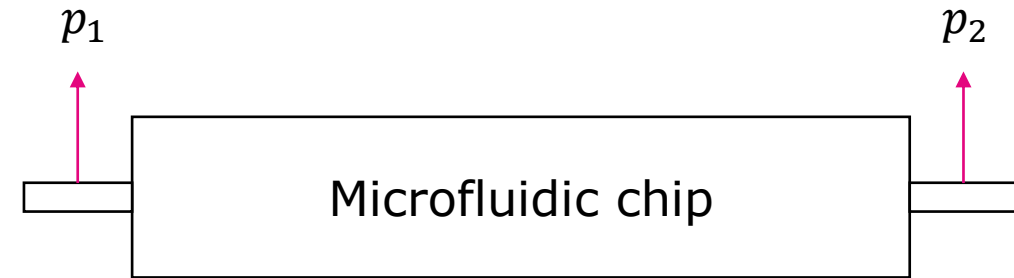
$$\bar{w} = \frac{\Delta p c^2}{\mu L} \left[\frac{1}{3} - \frac{64}{\pi^5} \frac{c}{b} \tanh \left(\frac{\pi b}{2c} \right) \right]$$

- Values:
 - Semi-axes b (major), c (minor), $b \geq c$
 - Δp pressure drop; $p_1 - p_2$ ($p_1 \geq p_2$)
 - L : channel length [m]
 - ϵ : aspect ratio; $\epsilon = \frac{c}{b}$



$$A = 4bc$$

$$P = 4(b + c)$$



w : flow velocity $\left[\frac{m}{s}\right]$

p : pressure [Pa]

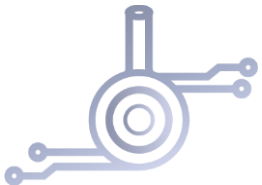
μ : dynamic viscosity [Pa · s]

FLOW CONTROL IN MICROFLUIDICS

- Flow rate: $Q = w \cdot A$ unit: $\left[\frac{m^3}{s}\right]$
- Liquid pumps (later lecture) are not perfect flow rate generators
- Back pressure Δp_{back} lowers flow rate Q :

$$Q = Q_{max} \cdot \frac{\Delta p_{max} - \Delta p_{back}}{\Delta p_{max}}$$

- Where:
 - Q_{max} is the flow rate when nothing's attached to the pump
 - Δp_{max} is the maximum backpressure the pump can take (find in specifications)





PRESSURE AND FLOW RATE IN MICROCHANNELS

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EXAMPLE: DROPLET GENERATION

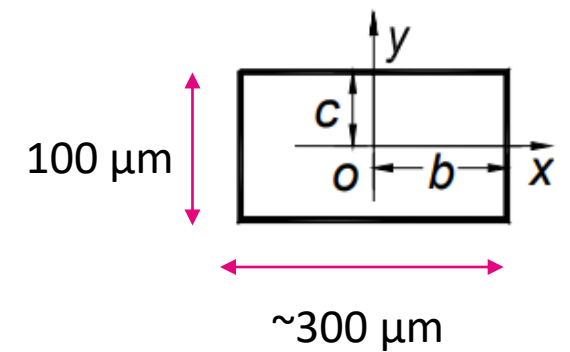
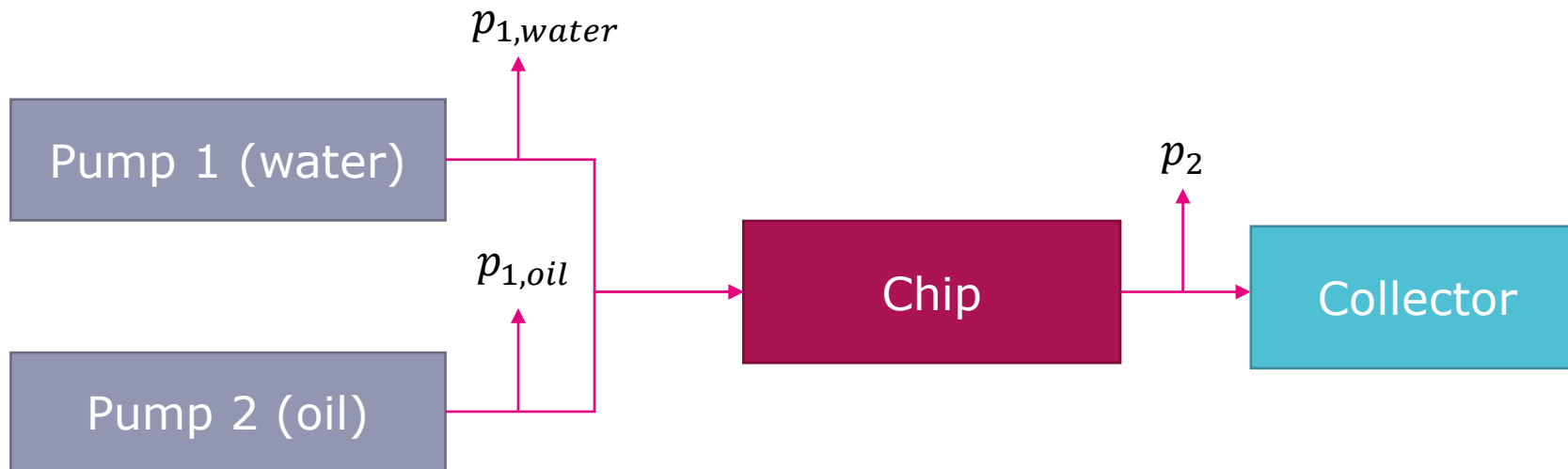
- 2 pumps
- 1 microfluidic chip (rectangular channels)
- 3 pressure sensors are needed, 2 on each flow path before the chip and 1 on the output

$$\mu_{water} = 0.00089 \text{ Pa} \cdot \text{s}$$

$$\mu_{mineral\ oil} = \sim 0.080 \text{ Pa} \cdot \text{s}$$

$$c = 50\mu\text{m}; b = 150\mu\text{m}; L = 1\text{ cm}$$

$$\Delta p = 100 \text{ Pa}$$



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TAL TECH

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